Optimal Branching Asymmetry of Hydrodynamic Pulsatile Trees

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Most of the studies on optimal transport are done for steady state regime conditions. Yet, there exists numerous examples in living systems where supply tree networks have to deliver products in a limited time due to the pulsatile character of the flow, as it is the case for mammalian respiration. We report here that introducing a systematic branching asymmetry allows the tree to reduce the average delivery time of the products. It simultaneously increases its robustness against the inevitable variability of sizes related to morphogenesis. We then apply this approach to the human tracheobronchial tree. We show that in this case all extremities are supplied with fresh air, provided that the asymmetry is smaller than a critical threshold which happens to match the asymmetry measured in the human lung. This could indicate that the structure is tuned at the maximum asymmetry level that allows the lung to feed all terminal units with fresh air.

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Branched transportation networks are ubiquitous in living systems. Such trees have been suggested to allow efficient feeding of the body volume from a small source, the aorta for blood or the mouth for oxygen [1–7]. For example, the human tracheobronchial tree brings fresh air to the oxygen-blood exchange units, called the *acini*, that fill the majority of the volume of the thoracic cage [1].

In the general perspective of how statistical physics may help to better understand the relation between structure and physiological function, we focus here on pulsatile trees in which the delivery of products has to be achieved in a limited time. For example in mammalian respiration, the respiratory cycle is made in two successive steps, inspiration and expiration. The period of this cycle is about 5 seconds for humans at rest (2 s for inspiration, 3 s for expiration). And of course, the transit time from the mouth to the acini has to be short enough so that expiration does not start before the arrival of fresh air into the acini. The present work analyzes the possible statistical constraints related to this last condition.

From the point of view of ventilation, the conducting airway system can be modeled as an arrangement of pipes defined by their diameter and length. The branchings are essentially dichotomous, each airway being divided into two smaller daughter airways. A branching defines the beginning of a new generation. The tracheobronchial tree starts at the trachea (generation 0) and ends in the terminal bronchioles (around generation 15) at the entrance of the acini [1]. Since no gas exchanges take place in the tracheobronchial tree, its volume is referred to as the *dead space volume* (DSV). Its value is around 170 ml in the human lung [8]. To better understand human respiration in relation with the tree structure, we discuss successively the general properties of two models, respectively symmetric and asymmetric, before discussing the real human airway system.

The first model has symmetrical branching. Although the human airway system is both nonsymmetric and exhibits some type of randomness, a fundamental step in describing its morphology has been the introduction of the so called Weibel's "A" model [1]. In this first model, the tree is likened to a hierarchical network of cylindrical pipes with symmetrical branching and a uniform scaling ratio $h_0 = 2^{-1/3} \approx 0.79$ between the airway sizes of consecutive generations. This value corresponds to the classical Murray-Hess law [9,10] for which the diameter of the mother branch d_0 and the diameters of both daughter branches d_1 and d_2 are linked by the relationship $d_0^3 = d_1^3 + d_2^3$.

An important second step in modeling the human lung morphology has been the introduction from anatomical studies of a systematic asymmetry [11–15]. This is the second model studied in this Letter. The branching asymmetry is characterized by two different scaling ratios, $h_{0,\text{max}} = 0.88$ and $h_{0,\text{min}} = 0.68$ [15]. Each parent airway gives rise to a larger daughter airway (the major airway) and a smaller daughter airway (the minor airway). Note that $(0.88)^3 + (0.68)^3 = 1$ so that the asymmetric tree respects the above dissipation requirement. And so, the Weibel's A model is the exact symmetrization of the real asymmetric structure.

Those are the two models to be compared, including the possible role of a statistical noise associated to anatomical variability. Note that two different types of structural randomness can appear in these models: the first source of disorder, due to the systematic branching asymmetry, is found in the random succession of large and small airways along any given airway path. The second type of disorder (the variability) results from the statistical noise of the biological growth process [8] and spreads the distribution of the branch sizes at a given generation even in the symmetric model.

The criterion that will be used in the following to quantify the delivery performance of the tree is the distribution of oxygenation times of fresh air into the acini. The oxygenation time in one acinus is obtained by subtracting from the total duration of the inspiratory phase, t_{ins} , the time spent in the extrathoracic airways, t_{ext} (approximately constant and equal to 0.47 s at rest [16]), and the transit time from the trachea to this acinus, t_{tr} :

$$t_{\rm ox} = t_{\rm ins} - t_{\rm ext} - t_{\rm tr}$$

The performances of symmetric and asymmetric trees have been computed on 15-generation trees. The geometrical parameters used in our computations, are summarized in Table I. These are the scaling ratios at each generation and the length to diameter ratio for each generation. It has to be noted that the values of the dead space volumes are kept almost similar. Because of the uniform motion of the thoracic cage, each acinus is assumed to act as a hydrodynamic pump draining the same flux. In other terms, the gas exchange units are equitably ventilated [17]. As a consequence, starting from the bottom of the tree, any two daughters of a given mother branch create, independently of their sizes, the same additive flux in their mother branch. The time spent in a branch is then directly obtained from the flux and the branch size. Thus, in both laminar and turbulent regimes, the transit time across the tree is determined by the flux prescribed in the acini only. In the inspiratory phase studied here, the total flow can be considered approximately constant in time with a velocity in the trachea of about 1 m/s [8]. Since the duration of the inspiration t_{ins} and the time spent in the extrathoracic airways t_{ext} are the same for all acini, the oxygenation times in the acini are thus entirely determined by the transit times of fresh air from the trachea to the terminal bronchioles.

Figure 1 shows the distribution of the acini oxygenation times for both models. The distribution for the symmetric tree trivially presents a single peak at t = 0.67 s as all pathways from the trachea to a terminal bronchiole are identical. The distribution of oxygenation times for the asymmetric tree is spread around a mean value of 0.82 s and has a standard deviation of 0.43 s. Therefore, on average, fresh air arrives slightly sooner and remains longer in acini supplied by an asymmetric tracheobronchial

TABLE I. Model parameters

Model	Scaling ratio for D	Ratio L/D^{a}	DSV (ml)
Symmetric Asymmetric	$h_0 = 2^{-1/3}$ $h_{0,\min} = 0.68$ $h_0 = 0.88$	3.00 3.00	220 213

^aD and L: diameter and length of the airway.

tree than by a symmetric one. (Such an asymmetric tree structure can be described as multifractal [18,19].)

We now study how the performances of these tree structures are robust or not with respect to anatomical variability. To mimic this variability, we introduce a "growth noise" by adding Gaussian variations of the scaling ratios. At each branching, the values of the scaling ratios are modified to become random variables:

$$h_{\min} = h_{0,\min} + \sigma X, \qquad h_{\max}^3 + h_{\min}^3 = h_{0,\max}^3 + h_{0,\min}^3$$
(1)

X being a centered Gaussian random variable of standard deviation 1. The mean values $h_{0,\min}$ and $h_{0,\max}$ of these random variables correspond to the values given in Table I. Scaling ratios of different bifurcations are assumed to be independent random variables while in the same branching, scaling ratios h_{\min} and h_{\max} are anticorrelated. This means that if the random variable for h_{\max} take a larger (resp. smaller) value than its mean value, then h_{\min} is very likely to take a smaller (resp. larger) value than its mean value.

The results are shown in Fig. 2 which displays the distributions of oxygenation times for both symmetric and asymmetric trees with randomized scaling ratios ($\sigma = 0.05$). The distribution for the symmetric tree is now also spread, with an average oxygenation time of 0.67 s and a standard deviation of 0.32 s. Unlike the symmetric case, the distribution in the asymmetric model is not modified by the randomization of the scaling ratios (mean value of 0.82 s and standard deviation of 0.44 s). The delivery of products through a dichotomous tree of constant depth thus appears to be more efficient both for average oxygenation time and immunity versus growth fluctuations.

So far, the two model trees that were considered had an equal number of generations for all pathways. In fact, the



FIG. 1. Distribution of oxygenation times in the acini for both symmetric (gray) and asymmetric (black) trees. All the pathways have the same transit times in the symmetric case, hence a single peak distribution of oxygenation times at 0.67 s. In the asymmetric case the distribution is spread with a mean value about 0.82 s and a standard deviation of 0.43 s.



FIG. 2. Distribution of oxygenation times with randomized scaling ratios according to Eq. (2): symmetric tree in gray and asymmetric tree in black. The oxygenation times are spread in the symmetric case, but the distribution is shifted towards smaller oxygenation times. The distribution for the asymmetric tree is not modified by randomization.

real human tracheobronchial tree is even more complex because not only the branchings are asymmetric but also the number of generations is not uniform [11,12,14]. The human tracheobronchial tree does not end at a constant generation but more at a constant airway diameter, that of the terminal bronchioles, around 0.5 mm [8,17]. The terminal generations of the tree range from 8 to 22 [11] and the length of the airways in the first generations also exhibits specific features linked to anatomical constraints [1,12,20]. The diameter scaling ratios are kept equal to 0.68 and 0.88 for all generations. The aspect ratios (length over diameter) are specific for the first 4 generations (respectively equal to 3.07, 1.75, 1.43, and 1.85) and equal to 3.00 for higher generations (generations 5 to 22). With these parameters, the distribution of oxygenation times for the real human tree (not shown here) is found to have an average oxygenation time of 0.67 s and a standard deviation of 0.13 s.

The asymmetry level, namely $h_{0,\text{max}} = 0.88$ and $h_{0,\min} = 0.68$, used in the above computations was considered as a given fact drawn from anatomical measurements. It is a natural question to ask for a reason for such values. For obvious reasons, the branching asymmetry cannot be too strong because it would lead to a structure with only very few wide pathways surrounded by a large number of much narrower pathways with large hydrodynamic resistances. Moreover, due to flux conservation, the wider pathways correspond to larger transit times. If the asymmetry level were too large, a number of extremities would not be supplied with fresh air because the transit time in their pathway would be too long. We will now investigate the influence of the asymmetry level on the acini oxygenation. The question that naturally arises is thus the following: How much asymmetry can there be? In other words, can one define an optimal asymmetry level?

In order to investigate this question, trees of different asymmetry levels have been studied. In this study, the asymmetry level is characterized by one parameter α such that:

$$h_{0,\max}^3 = h_0^3(1+\alpha), \qquad h_{0,\min}^3 = h_0^3(1-\alpha).$$
 (2)

The scaling ratios 0.88 and 0.68 as measured in the human tracheobronchial tree would for instance correspond to an asymmetry level of 36% ($\alpha = 0.36$). All computed trees are conditioned to have the same thoracic volume (dead space volume + acini volume) and the aspect ratios L/Dgiven above. Considering that fresh air has to remain at least 0.3 s in the acinar region in order to achieve the gas exchange process (a duration consistent with computations of the dynamical diffusion oxygen transport in the acinus [21]), we have computed for each asymmetry level the proportion of acini with an oxygenation time larger than 0.3 s. This corresponds to a total transit time from the mouth to the terminal bronchiole smaller than 1.7 s. Results are presented in Fig. 3. The proportion of acini fed with fresh air for more than 0.3 s is 100% for the symmetric tree (zero asymmetry level) and remains 100% until a threshold value of the asymmetry level. As one can see on Fig. 3, this threshold value is about 35%, almost identical to the value measured in the human tracheobronchial tree.

So it seems that the systematic asymmetry found in the tracheobronchial tree corresponds to the maximum value that allows the tree to feed all acini. There are several advantages to such a structure: 100% of the acini receive fresh air, and the distribution of the ventilated volumes is robust against anatomical variability. Also, the spread distribution of arrival times in the exchange units may contribute to smoothen the oxygen delivery to the blood. On the other hand, due to this distribution of transit times, all acini do not receive the same volume of fresh air. Even if all acini receive the same flux, the unevenness of branching creates an inhomogeneity of the volumes of supplied fresh air that multiplicatively increases at each generation. In the limit of an infinite tree, this would mathematically lead to a



FIG. 3 (color online). Proportion of inactive acini (with oxygenation time smaller than 0.3 s) as a function of the asymmetry level α . All acini are found to be active provided that the asymmetry level is below $\alpha \approx 35\%$. This value almost exactly corresponds to the measured asymmetry level in the human lung (36%).



FIG. 4 (color). 2D representation of the distribution of volumes of fresh air delivered at generation 10 in the human tracheobronchial tree (parameters described in the text).

multifractal distribution of the volume of fresh air delivered in the extremities [22]. This pre-multifractal behavior can be observed in Fig. 4 which shows a 2D representation of the distribution of volumes of fresh air delivered at generation 10. One observes a wide spread of the distribution of fresh air volumes. This could indicate that a dynamical regulation of airway diameters might be necessary to minimize such effects, as already suggested to fight inertial effects in the upper part of the airway tree [23]. Note that the spread in the distribution of external gas in the acini would also induce an inherent noise in NMR imaging of the lung.

In summary, numerical computations show that symmetric branching trees are not optimal to supply a volume when a constraint of limited delivery time is imposed. For trees of uniform depth, the average transit time is found to be smaller when the branching is asymmetric rather than symmetric. Moreover, the distribution of oxygenation times in the acini of the asymmetric tree is almost not modified by a stochastic variability of the sizes of the branches. This approach is then extended to the study of the role of variable asymmetry in trees, with the same trachea, the same ratio length over diameter, the same diameter of the terminal bronchioles and the same inner volume. It is shown then that there exists a maximum asymmetry level above which the number of terminal units, or acini, supplied with fresh air, departs from 100%. Interestingly, this maximum value almost exactly corresponds to the asymmetry level measured in the human lung. The geometry of the lung airways thus appears as if being adjusted to have the largest possible branching asymmetry, while still being able to feed efficiently all acini with fresh air. It may be considered as remarkable that an asymmetric tree works better and that the natural selection of mammals seems to have found a level of asymmetry that can be considered as best from the physical point of view. The authors would like to thank Professor E. R. Weibel for fruitful discussions.

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- E. R. Weibel, *Morphometry of the Human Lung* (Springer-Verlag, Berlin Heidelberg and Academic Press, New York, 1963).
- [2] G.B. West, J.H. Brown, and B.J. Enquist, Science 276, 122 (1997).
- [3] B. Mauroy, M. Filoche, E. R. Weibel, and B. Sapoval, Nature (London) 427, 633 (2004).
- [4] M. Bernot, V. Caselles, and J.-M. Morel, *Optimal Transportation Networks: Models and Theory* (Springer-Verlag, Berlin Heidelberg, 2008).
- [5] B. Mauroy and P. Bokov, Phys. Biol. 7, 016007 (2010).
- [6] P.S. Dodds, Phys. Rev. Lett. **104**, 048702 (2010).
- [7] F. Corson, Phys. Rev. Lett. 104, 048703 (2010).
- [8] E. R. Weibel, *The Pathway for Oxygen* (Harvard University Press, Cambridge, 1984).
- [9] W.R. Hess, Archiv fur Physiologie 12, 1 (1914).
- [10] C.D. Murray, Proc. Natl. Acad. Sci. U.S.A. 12, 207 (1926).
- [11] K. Horsfield, G. Dart, D. E. Olson, G. F. Filley, and G. Cumming, J. Appl. Physiol. **31**, 207 (1971).
- [12] O.G. Raabe, H.C. Yeh, G.M. Schum, and R.F. Phalen, Tech. Rep. Publ. Report No. LF-53, 1976.
- [13] C.G. Phillips and S.R. Kaye, Respir. Physiol. 107, 85 (1997).
- [14] H. Kitaoka, R. Takaki, and B. Suki, J. Appl. Physiol. 87, 2207 (1999).
- [15] A. Majumdar, A. M. Alencar, S. V. Buldyrev, Z. Hantos, K. R. Lutchen, H. E. Stanley, and B. Suki, Phys. Rev. Lett. 95, 168101(2005).
- [16] J. Sandeau, I. Katz, R. Fodil, B. Louis, G. Apiou-Sbirlea, G. Caillibotte, and D. Isabey, J. Aerosol Sci. 41, 281 (2010).
- [17] E.R. Weibel, B. Sapoval, and M. Filoche, Respir. Physiolo. Neurobio. **148**, 3 (2005).
- [18] M. Zamir, J. Theor. Biol. 212, 183 (2001).
- [19] A. Schmidt, S. Zidowitz, A. Kriete, T. Denhard, S. Krass, and H. O. Peitgen, Comput. Med. Imaging Graph. 28, 203 (2004).
- [20] C.G. Phillips and S.R. Kaye, Respir. Physiol. 102, 303 (1995).
- [21] M. Filoche, A.A. Moreira, J.S. Andrade, Jr., and B. Sapoval, Advances in Experimental Medicine and Biology 605, 167 (2008).
- [22] B. Sapoval, *Universalités et Fractales* (Flammarion, Paris, 1997), pp. 164–165.
- [23] B. Mauroy, M. Filoche, J. S. Andrade, Jr., and B. Sapoval, Phys. Rev. Lett. **90**, 148101 (2003).